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*Sound Light: photoacoustic
imaging of cancer*

Wiendelt Steenbergen
MIRA institute / Biomedical Photonic Imaging Group



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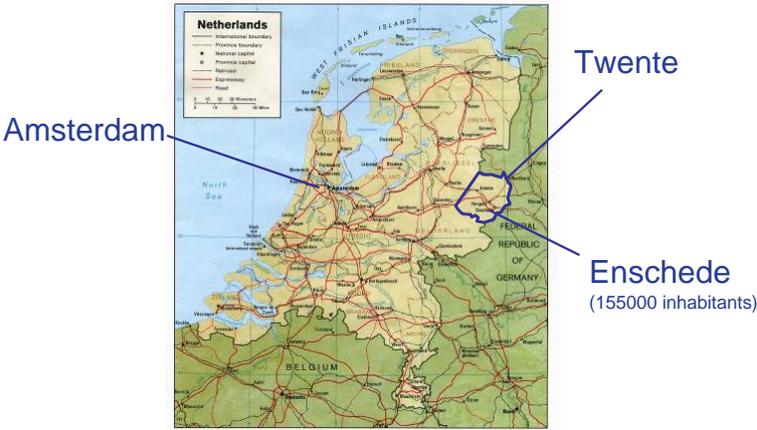
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Biomedical Photonic Imaging group



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Geography



www.lib.utexas.edu/maps/europe/netherlands_rel87.jpg

Enschede

1826



1916



2008

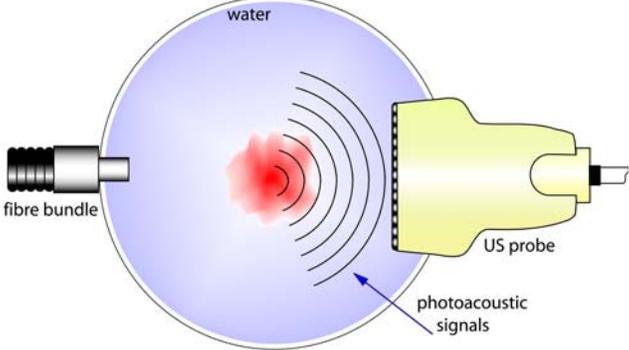


<http://www.enschede-stad.nl>

Enschede



Photoacoustic Imaging



$$p = \Gamma \mu_a \Phi(x, y, z)$$



Overview of tumor imaging studies

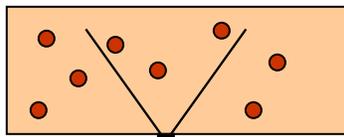
Animals:

- Vascularisation during tumor growth

Humans:

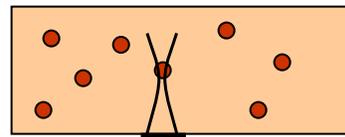
- PA Mammography

Detection geometries



Wide angle detection

- Reconstruction needed
- + Can be made into array



Focussed detection

- + No reconstruction needed
- Cannot be made into array



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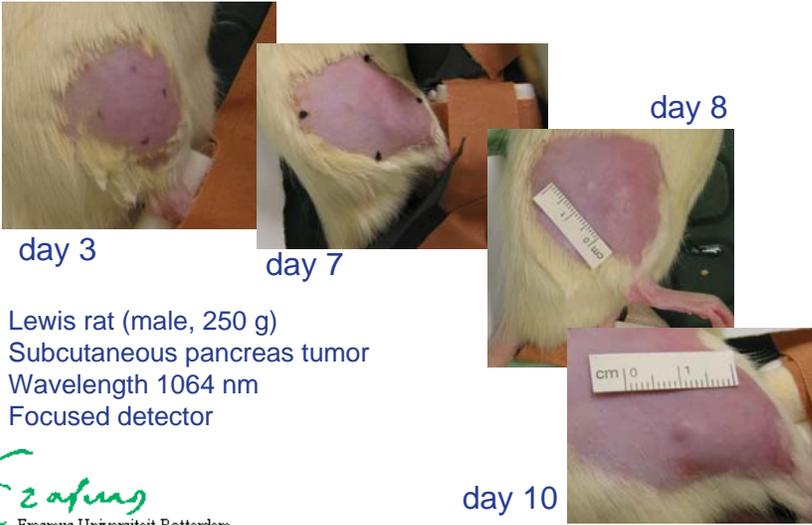
Photoacoustic imaging of subcutaneous tumor

- Lewis rat (male, 250 g)
- 8×10^6 pancreas tumor cells injected subcutaneously in hind limb
- Measurements on day 3, 7, 8 and 10 (tumor injected on day 1)
- Wavelength 1064 nm
- Pulse duration 14 ns
- Pulse energy 2 mJ
- **Focussed and unfocussed detector**

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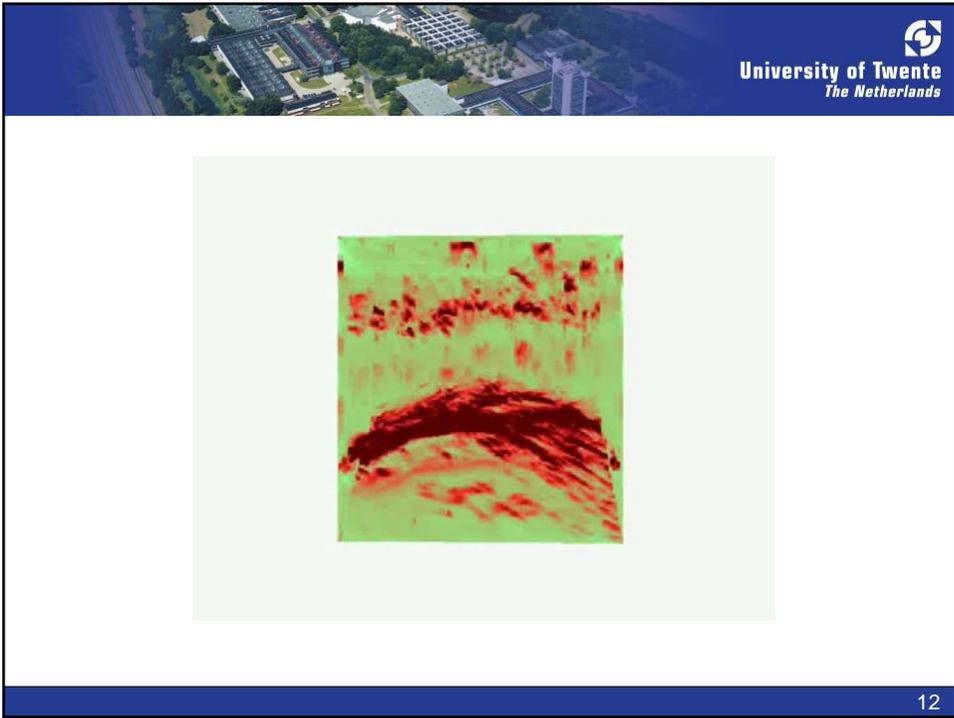
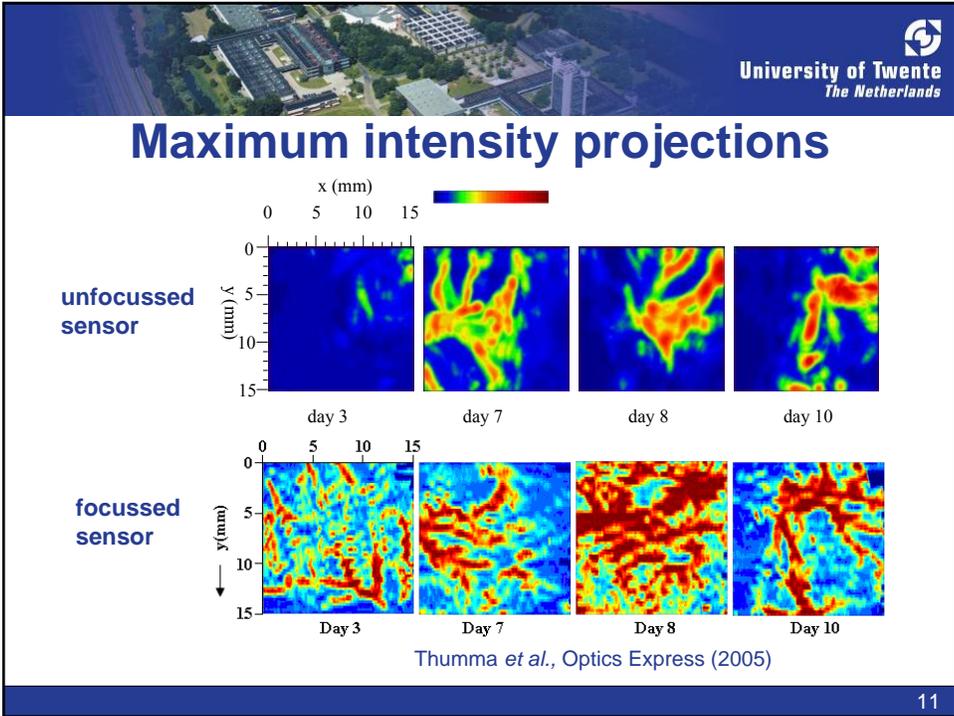


day 3 day 7 day 8 day 10

- Lewis rat (male, 250 g)
- Subcutaneous pancreas tumor
- Wavelength 1064 nm
- Focused detector

Erasmus
Erasmus Universiteit Rotterdam

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Overview of tumor studies

Animals:

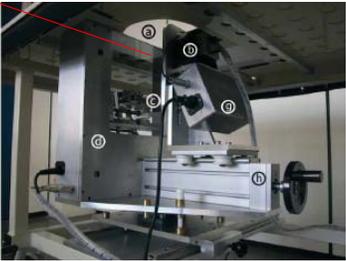
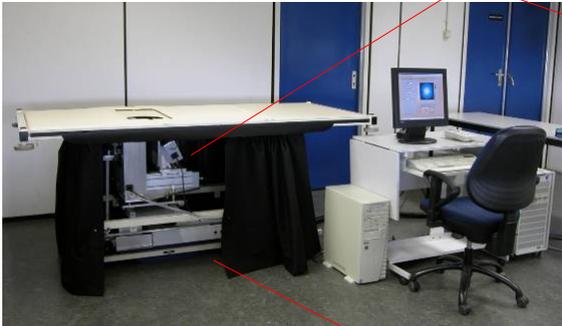
- Vascularisation during tumor growth

Humans:

- PA Mammography

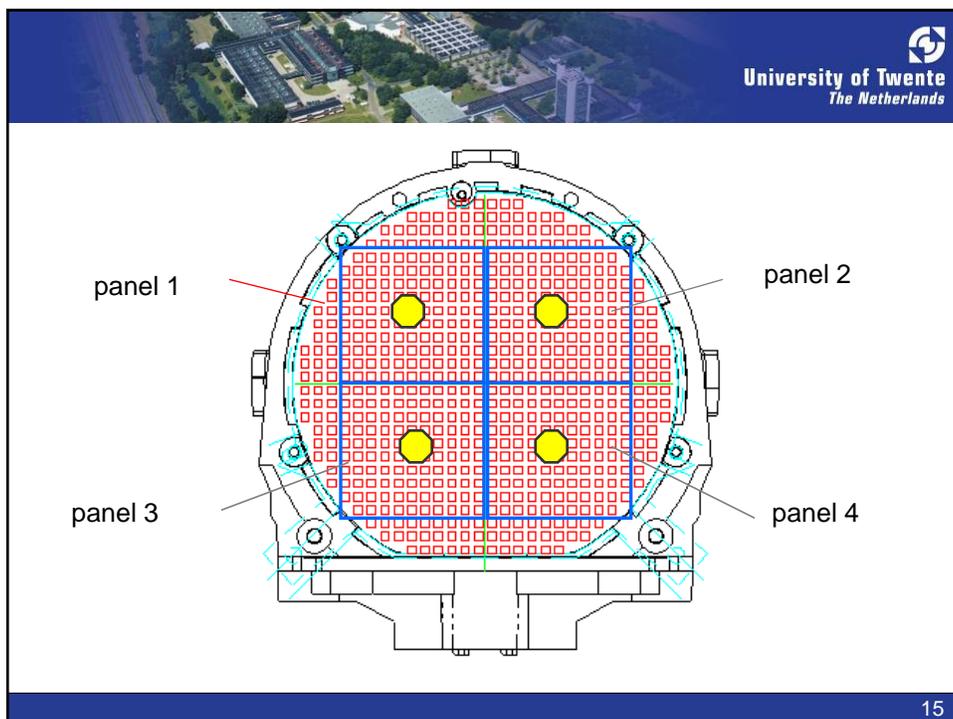
The Photoacoustic Mammoscope 1 (PAM1)

ultrasound detection array, 1 MHz



ND-YAG laser, 1064 nm, pulse energy 60 mJ

Phys. Med. Biol. (2005)



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Photoacoustic mammography pilot study

- Inclusion criteria
 - Palpable lump
 - X-ray and US: high suspicion for malignancy
 - Pre-selected by clinician for high probability of detection
 - Subjects in good general health (45 minutes exam)
 - Of legal age; fully competent to give informed consent etc
- Exclusion criteria
 - Patients with history of surgical biopsies

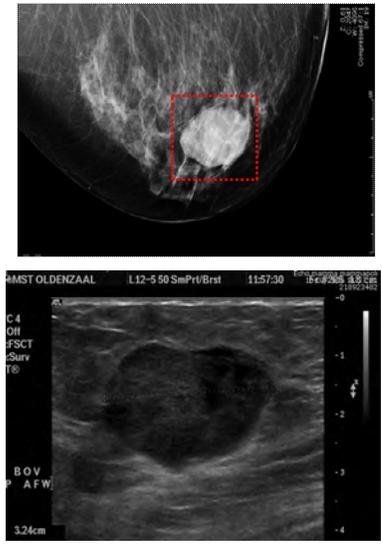
Manohar *et al.*, *Optics Express* (2007)

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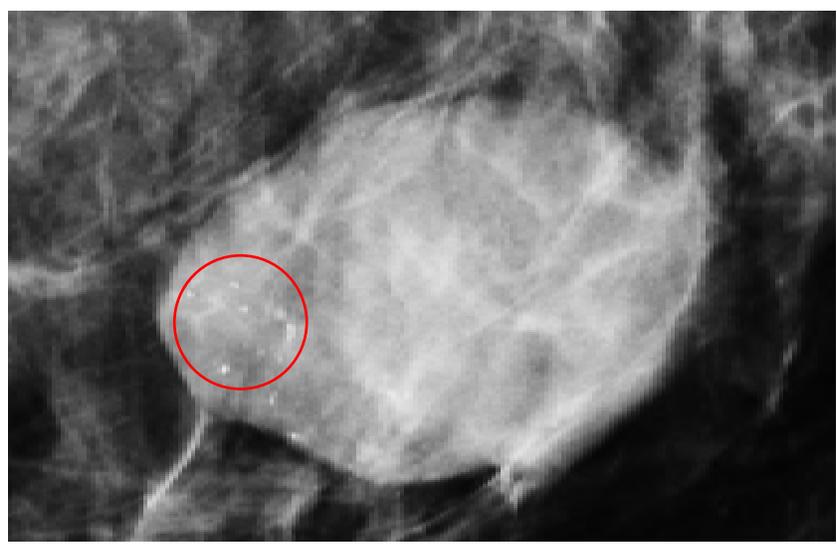
Case

- 57 year, Caucasian
- Palpable lump central in right breast
- Carcinoma with neuroendocrine differentiation
- ROI photoacoustic scan: 43x46 mm
- Breast thickness in scanner: 59.5 mm



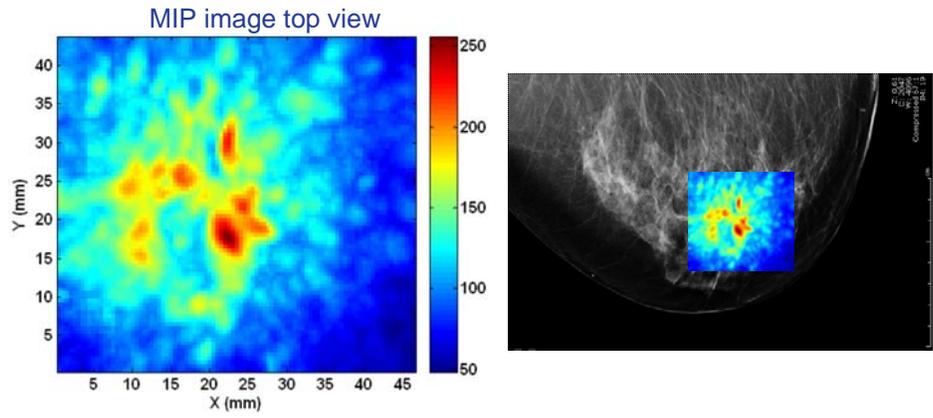
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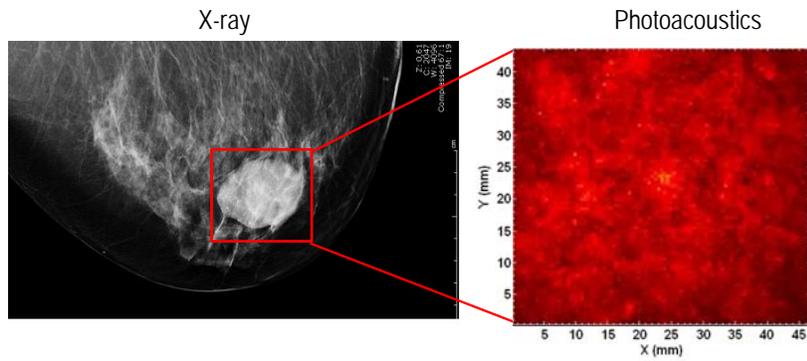
Optics Express (2007)



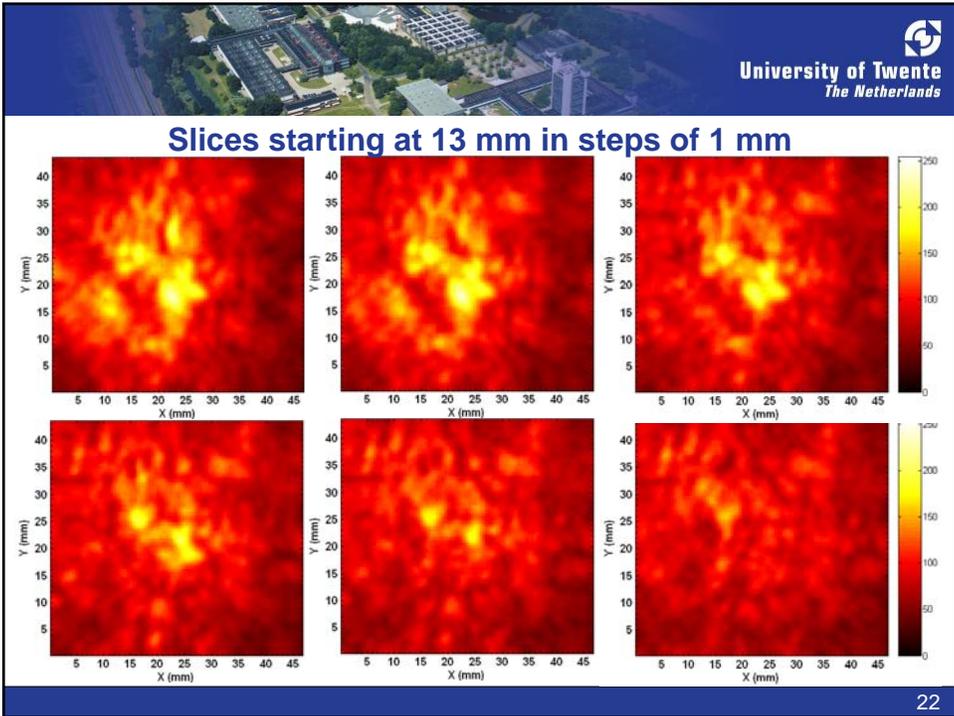
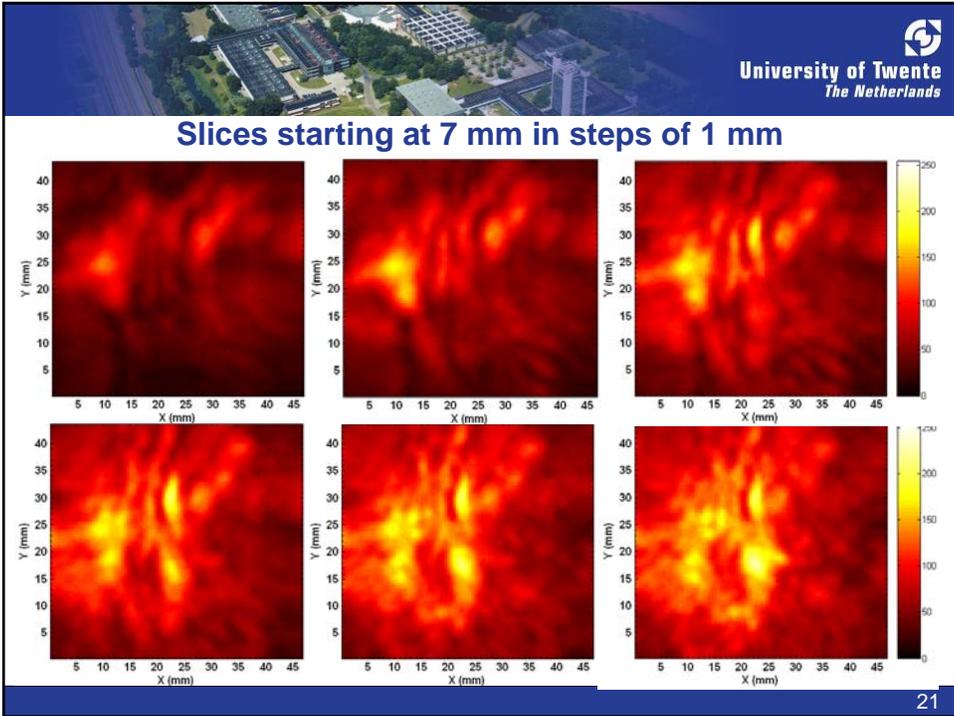
Carcinoma

Pathology: tumor size = 26 mm

Photoacoustics: tumor size = 25 x 32 mm



Steps of $\frac{1}{4}$ mm,
from 20 to 5 mm depth





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Photoacoustics, current status

Capabilities of PA shown *in vivo* for

- Imaging of implanted subcutaneous tumors
 - Resolution: 100-150 μm
 - Measurement depth: 5 mm

- Breast imaging
 - Instrumental resolution 3 mm
 - Measurement depth 15-20 mm (128 averages)

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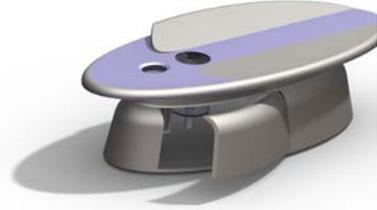
Needs for better photoacoustics

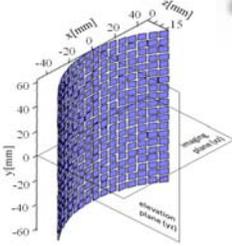
- faster imaging
 - Parallel signal acquisition (money)
- more quantitative imaging
 - More signals for better image reconstruction
 - Cope with acoustic tissue inhomogeneities
 - Measure absolute concentration of substances

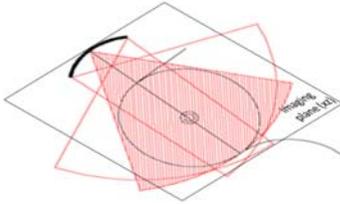
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PAM2: from flat plate to tomography







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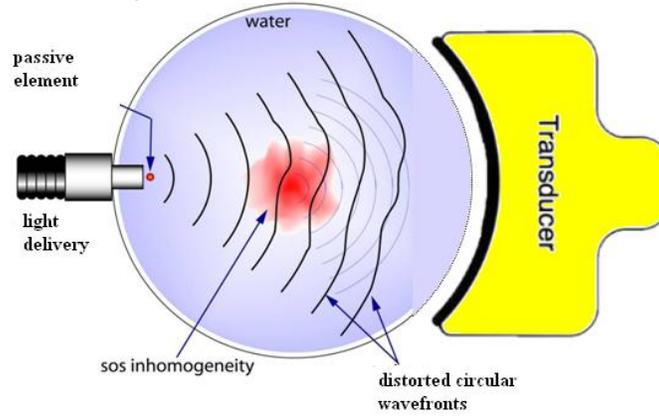
Needs for better photoacoustics

- faster imaging
 - Parallel signal acquisition (money)
- more quantitative imaging
 - More signals for better image reconstruction
 - **Cope with acoustic tissue inhomogeneities**
 - Measure absolute concentration of substances

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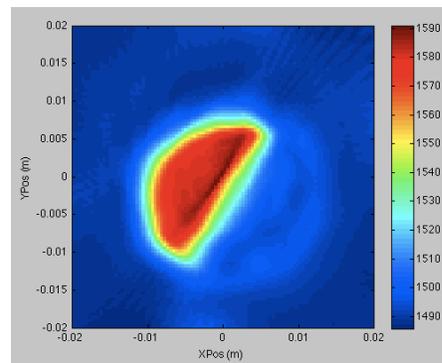
Imaging of acoustic parameters

Speed of sound and attenuation



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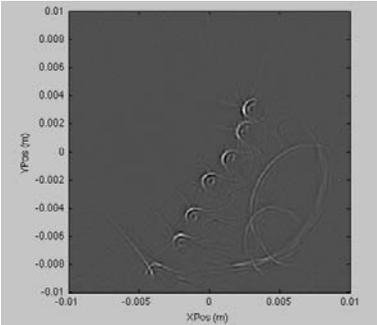
PVA inclusion in an agar phantom



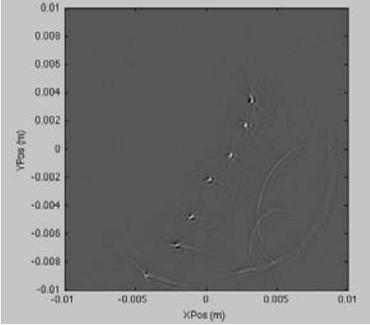
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Effect of assumed speed of sound on PA image

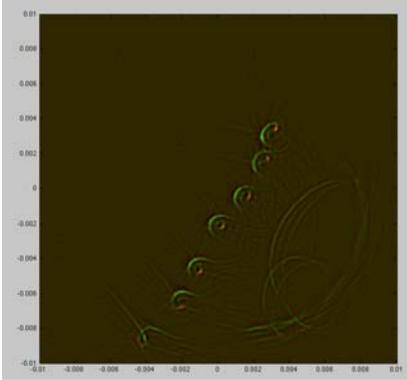
Assumed SOS=1490 m/s

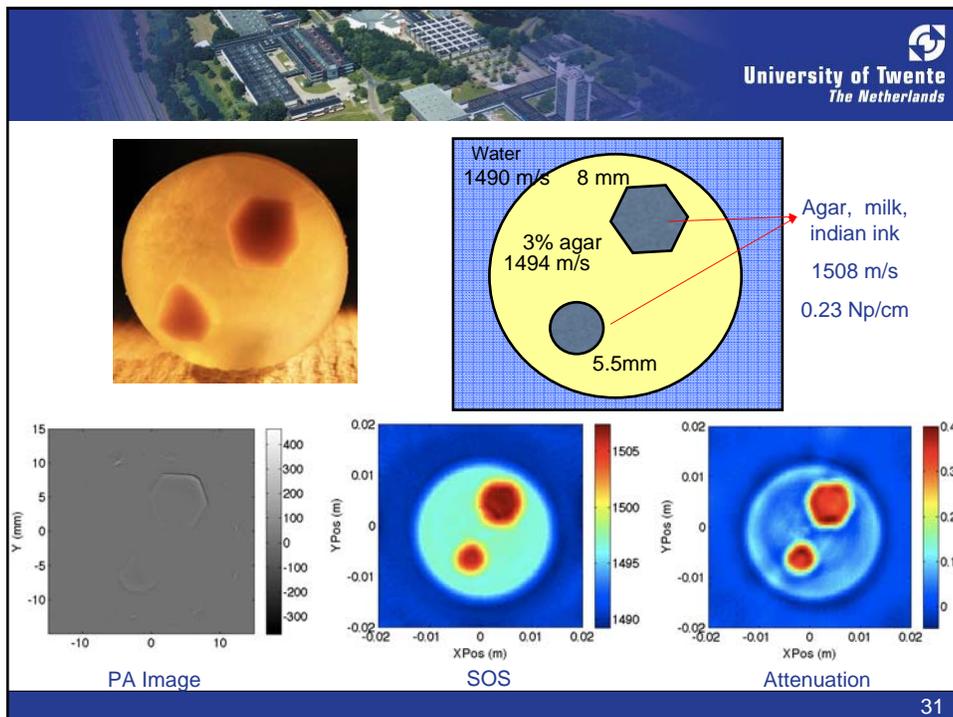


Using measured SoS map



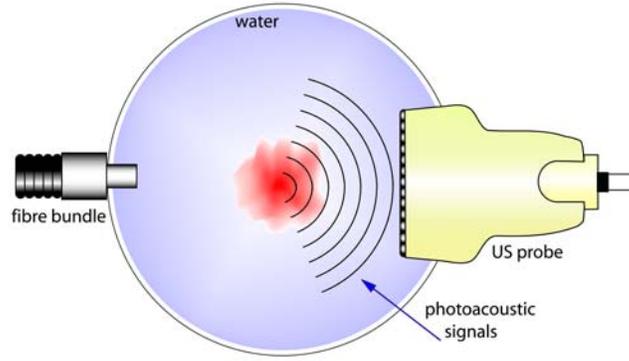
Effect of assumed speed of sound on PA image





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- ## Needs for better photoacoustics
- faster imaging
 - Parallel signal acquisition (money)
 - more quantitative imaging
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 - Cope with acoustic tissue inhomogeneities
 - Measure absolute concentration of substances
- 32

Photoacoustic Imaging



$$p = \Gamma \mu_a \Phi(x, y, z)$$



Tissue is a pinball machine



BSc thesis H.E. van Herpt



The quantification problem of photoacoustics

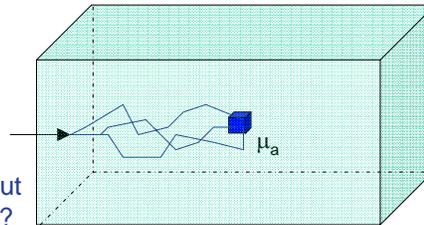
Initial pressure in absorbing volume after laser pulse:

$$P_0 = \Gamma \mu_a \Phi(x, y, z) ?$$

Γ : Grueneisen coefficient

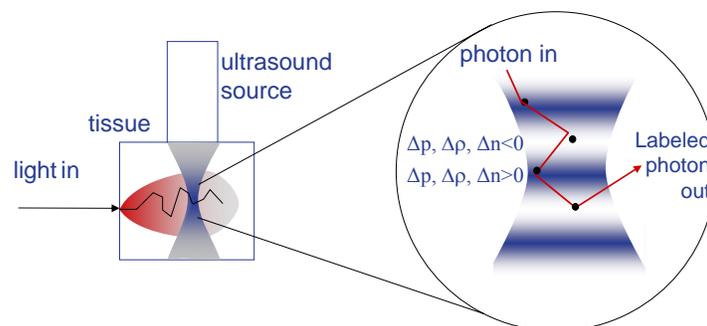
$\Phi(x, y, z)$: Fluence

Can we estimate absolute absorption coefficients without using a light transport model?



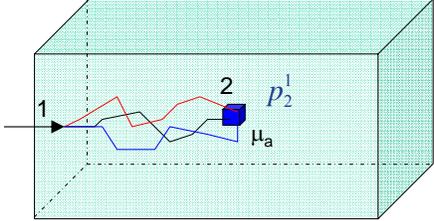
Yes

Principle 2: labeling of light acousto-optic modulation

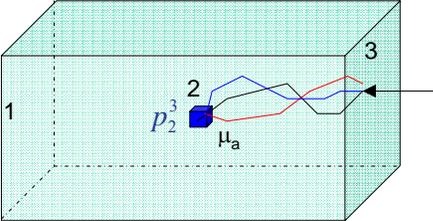



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Step 1: PA excitation in point 1 and 3



$p_2^1 = \Gamma \mu_a \Phi_2^1$
 $\Phi_2^1 = \text{fluence}$



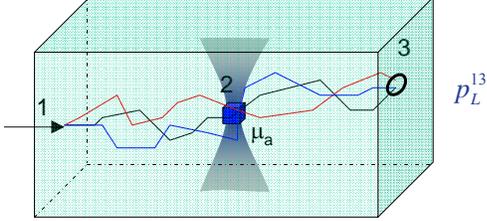
$p_2^3 = \Gamma \mu_a \Phi_2^3$

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Step 2: label the light

inject in 1, label in 2, detect in 3



p_L^{13}

Amount of labeled light detected in 3:

$$p_L^{13} \propto \text{Pr}(1,2,3) \propto \text{Pr}(1,2) \text{Pr}(2,3) \propto \text{Pr}(1,2) \text{Pr}(3,2) \propto \Phi_2^1 \Phi_2^3$$

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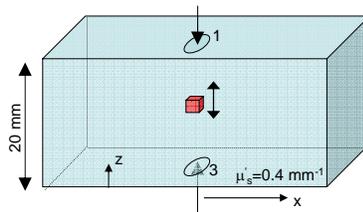
Step 3: combining measurements

$$\left. \begin{aligned} p_2^1 &= \Gamma \mu_a \Phi_2^1 \\ p_2^3 &= \Gamma \mu_a \Phi_2^3 \\ p_L^{13} &\propto \Phi_2^1 \Phi_2^3 \end{aligned} \right\} \text{3 equations, 3 unknowns}$$

$$\mu_a = c \sqrt{\frac{p_1 p_3}{p_L^{13}}}$$

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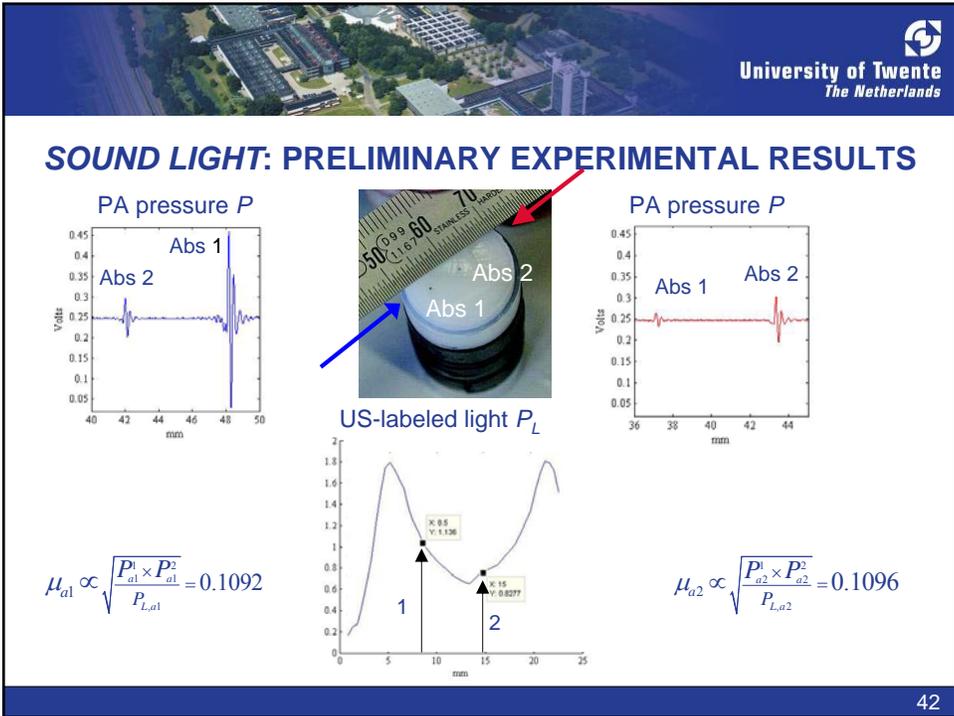
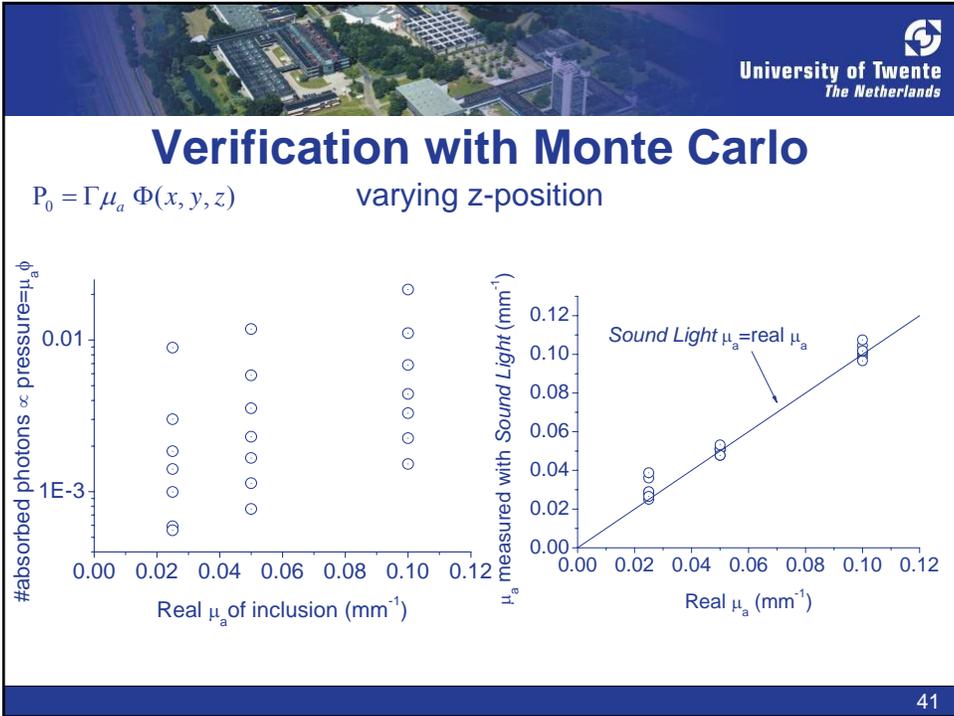
Verification with Monte Carlo



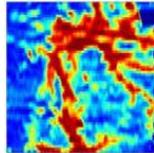
- 2D slab, thickness 20 mm
- Single absorbing inclusion: $\mu_a = 0.025, 0.05$ and 0.1 mm^{-1}

Position variations for the absorbing inclusion:
At fixed $x=y=0$: $4 < z < 16 \text{ mm}$

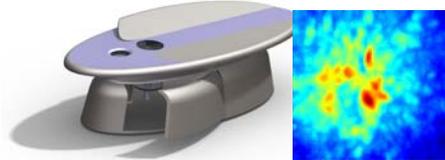
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SOUND LIGHT IN ONCOLOGY



PAM2, PAM3...



Research: quantification of

- neovascularisation
- smart contrast agents
- local drug delivery
- molecular processes

Clinical: mammography

- screening
- diagnosis
- monitoring of therapy

Acknowledgments

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